

Smoking and Intracranial Aneurysm Morphology

Allen L. Ho, MD*‡

Ning Lin, MD§

Kai U. Frerichs, MD*‡

Rose Du, MD, PhD*‡

*Department of Neurosurgery, Brigham and Women's Hospital, Boston, Massachusetts; ‡Harvard Medical School, Boston, Massachusetts; §Department of Neurological Surgery, New York-Presbyterian Hospital/Weill Cornell Medical Center, New York, New York

Correspondence:

Rose Du, MD, PhD,
Department of Neurosurgery,
Brigham and Women's Hospital,
75 Francis Street,
Boston, MA 02115.
E-mail: rdu@partners.org

Received, November 15, 2014.

Accepted, February 9, 2015.

Published Online, April 2, 2015.

Copyright © 2015 by the
Congress of Neurological Surgeons.

BACKGROUND: Smoking is a well-known independent risk factor for both aneurysm formation and rupture. There is mounting evidence that aneurysm morphology beyond size can have a significant role in aneurysm formation and rupture risk by its effects on aneurysmal hemodynamics.

OBJECTIVE: To study the variation in aneurysm morphology between smokers and nonsmokers and delineate how changes in these factors might affect aneurysm formation and rupture.

METHODS: We generated 3-dimensional models of aneurysms and their surrounding vasculature by analyzing preoperative computed tomography angiograms with Slicer software. We then examined the association between smoking status and intrinsic, transitional, and extrinsic aspects of aneurysm morphology in both univariate and multivariate statistical analyses.

RESULTS: From 2005 to 2013, 199 cerebral aneurysms in never smokers and current smokers were evaluated/treated at a single institution with available computed tomography angiograms (102 in never smokers and 97 in current smokers). Multivariate analysis of current smokers vs never smokers demonstrated that aneurysms in current smokers were significantly associated with multiple aneurysms (odds ratio [OR]: 2.15, $P = .03$), larger daughter vessel diameters (OR: 3.13, $P = .01$), larger size ratio (OR: 1.78, $P = .01$), and location at the basilar apex (OR: 6.26, $P = .02$).

CONCLUSION: The differences in aneurysm morphology between smoking and non-smoking patient populations may elucidate the effects of smoking on aneurysm formation and eventual rupture. We identified several aspects of aneurysm morphology significantly associated with smoking status that may provide the morphological basis for how smoking leads to increased aneurysm rupture.

KEY WORDS: Aneurysm, Fluid dynamic, Morphology, Smoking

Neurosurgery 77:59–66, 2015

DOI: 10.1227/NEU.0000000000000735

www.neurosurgery-online.com

The number of incidentally discovered intracranial aneurysms continues to increase with the increased use of cranial imaging,¹ and unruptured aneurysms now occur in nearly 3% of the general population.² Smoking has been implicated as an independent risk factor for both intracranial aneurysm formation^{3–5} and rupture.^{4,6,7} In population-based and cohort studies, nearly 75% of patients with aneurysmal subarachnoid hemorrhage have a history of smoking, and 50% to 60% are current smokers.^{8,9} Several prospective cohort studies have shown that smoking was also a predictor of de novo

aneurysm formation as well as increased rates of aneurysm growth.^{3–5} However, there remains no clear mechanism for aneurysm formation and rupture as a function of smoking status, although there have been several biochemical and biomechanical theories proposed.^{10–13}

Smoking has been shown to exacerbate atherosclerotic disease and to damage blood vessels in a predictable fashion, including injury to endothelial cells, occlusion of vasa vasorum, and interruption of elastin and collagen synthesis, that could lead to aneurysm genesis and rupture.^{11,12,14} It has also been shown that alterations in wall shear stress play a role in the initiation and rupture of intracranial aneurysms, although contradictory evidence has been offered regarding the direction of correlation of such a relationship.^{15–19} Smoking, along with hypertension, the other

ABBREVIATIONS: ACoA, anterior communicating artery; PCoA, posterior communicating artery; MCA, middle cerebral artery

well-known aneurysmal risk factor, leads to increased blood viscosity and concomitant alterations in wall shear stress that may affect aneurysm formation and rupture.^{20,21} There is now increasing evidence to suggest that aneurysm morphology beyond the predominant parameter of size used in clinical practice today has a profound effect on aneurysmal hemodynamics such as wall shear stress and a role in the clinical evaluation of aneurysm rupture risk.²²⁻²⁸ To date, no one has studied the variation in aneurysm morphology between smokers and nonsmokers and how these 2 factors may interact to affect aneurysm rupture. Our study was designed to identify the significant differences in aneurysm morphology between smokers and nonsmokers and delineate how these factors might affect rupture risk in these patients.

METHODS

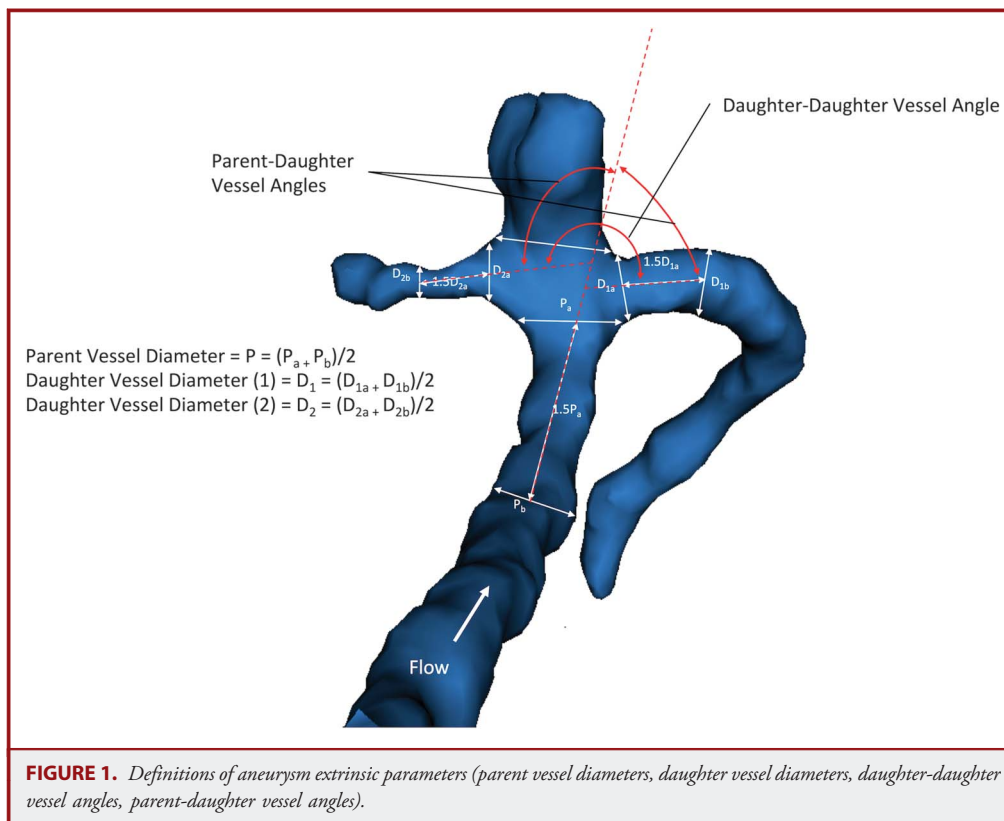
Patient Selection

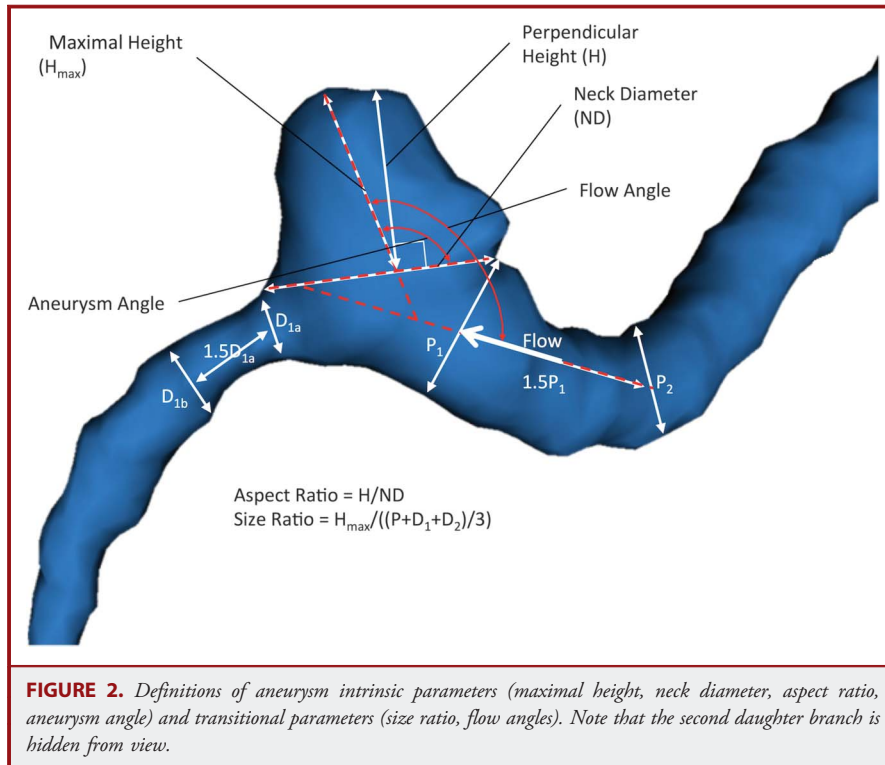
The study population consisted of patients with intracranial aneurysms evaluated and/or treated at the Brigham and Women’s Hospital during an 8-year period between 2005 and 2013 who were never smokers or current smokers. Patients with aneurysms that underwent reoperation, aneurysms that were associated with arteriovenous malformations, and aneurysms that lacked preoperative computed tomography (CT) angiograms were not included in the study. The anterior communicating artery (ACoA), posterior communicating artery (PCoA), and middle cerebral artery (MCA) aneurysm cohorts were consecutively treated patients, whereas

the basilar apex aneurysm cohort was composed of consecutive patients who were evaluated and/or treated. Medical records for these patients were queried for the relevant demographic and clinical information. Smoking history was defined as current smoker vs never. To avoid the heterogeneity present in the group of former smokers, only current smokers and never smokers were evaluated. In addition to smoking history, we also collected information on other risk factors commonly associated with aneurysm development and rupture including family history, presence of multiple aneurysms, history of hypertension, and history of aneurysm rupture. The study was approved by our institutional review board.

Reconstruction of 3-Dimensional Models

To conduct the morphological analysis of the aneurysms in our study, we deployed 3-dimensional (3-D) Slicer software (referred to as Slicer in the following text),^{29,30} an open-source, multiplatform visualization and image analysis software, as described previously.²² We created composite 3-D models of the aneurysms and their surrounding vasculature using preoperative CT angiography images. All CT angiograms were obtained using a SOMATOM Definition scanner (Siemens Medical Solutions USA, Malvern, Pennsylvania) with a slice thickness of 0.75 mm and increments of 0.5 mm. We were able to isolate the vascular compartment via thresholding. A triangle reduction and smoothing algorithm reconstructed the aneurysm borders and contours and generated a 3-D surface model of the aneurysm and surrounding vasculature that could be freely manipulated in the Slicer environment (Figures 1 and 2). Fiducial-based tractography enabled manual measurement of the volumes, lengths, and angles of the aneurysm and associated vessels.





Definition of Morphological Parameters

Aneurysm intrinsic, transitional, and extrinsic morphological parameters have been studied at length to assess their effects on rupture risk.^{14-18,23-27} Aneurysm intrinsic parameters are those that are intrinsic to the aneurysm morphology and include aneurysm size, volume, aspect ratio, and aneurysm angle.^{22-26,31-34} Transitional parameters are those that characterize the relationship between the aneurysm and its surrounding vasculature. Finally, aneurysm extrinsic parameters are those that are independent of the aneurysm and involve the surrounding vasculature as defined in our previous studies, such as parent-daughter vessel angle and daughter-daughter vessel angle.^{22,25,26}

Intrinsic Aneurysm Parameters

1. Aneurysm maximal height is the largest cross-sectional diameter of the aneurysm measured from the base of the aneurysm.^{31,35,36}
2. Aspect ratio is the ratio of the maximal perpendicular height of the aneurysm to the average neck diameter of the aneurysm.^{32,33,37}
3. Volume is the calculated volume of the 3-D aneurysm models.
4. Aneurysm angle is the angle formed between the plane of the neck of the aneurysm and the vector of the maximal height of the aneurysm. The aneurysm angle captures the angle of inclination of the aneurysm from the base of the neck.³²

Transitional Aneurysm Parameters

Transitional and extrinsic aneurysm parameters that incorporated the morphology of the surrounding vasculature were also included in our study. The parent vessels were defined as the source of blood flow into the aneurysm,

and daughter vessels were those that carry blood flow away from the aneurysm. Parent vessel data did not include ACoA aneurysms because many had 2 parent vessels. Similarly, daughter vessel analysis excluded some PCoA aneurysms because the PCoA is frequently not visualized on a CT angiogram.

1. Size ratio is the ratio between the maximal aneurysm height and mean vessel diameters of all vessel branches associated with the aneurysm. The mean vessel diameter of a particular vessel is determined by averaging the diameter of the cross section of the vessel at the neck of the aneurysm (D_1) with the diameter of the cross section at $1.5 \times D_1$ distance from the neck of the aneurysm. This mean vessel diameter was calculated for all vessels involved with the aneurysm and then averaged to generate the composite mean vessel diameter used to calculate the size ratio.^{32,38} Finally, the 2 center points of the vessel cross sections created in the size ratio measurement were connected to represent vessel vectors of flow in vessel angle measurements.
2. Flow angle is the angle formed between the vector of the maximal height of the aneurysm and the vector of flow through the parent artery. This angle captures the angle at which the aneurysm deviates in its formation from the vector of flow through the parent vessel.^{39,40}

Extrinsic Aneurysm Parameters

1. Vessel diameter is the diameter of the respective vessel most proximal to the aneurysm neck. Given that vessel and vessel diameters varied significantly between aneurysms in different locations, these measured vessel diameters were also normalized by the mean for each location subtype of aneurysm to adjust for any differences between absolute vessel sizes based on location. Both absolute and normalized values were included in our analysis.

2. Parent-daughter vessel angle is a composite mean of angles formed between the vector of flow of the parent artery and the vector of flow for each daughter artery.
3. Daughter-daughter vessel angle is the angle formed between each pair of daughter vessels.

Statistical Analysis

Demographic and clinical characteristics were analyzed for differences by smoking status using the χ^2 and 2-tailed *t* tests for binary and continuous variables, respectively. Univariate analysis was performed to compare the value of each morphological parameter between the smoking and nonsmoking groups. Multivariate logistic regression was also used to calculate the odds ratios (ORs) and 95% confidence intervals (CIs) for association with smoking status. Missing data were not removed from analysis. All statistical analyses were performed using JMP Pro 10, SAS version 9.2 (SAS Institute Inc, Cary, North Carolina) and R version 3.1.2 (R Foundation for Statistical Computing, Vienna, Austria).

RESULTS

From 2005 to 2013, 199 cerebral aneurysms in never smokers and current smokers were evaluated/treated at a single institution at which CT angiograms were available (102 never smokers, 97 current smokers). Demographic and clinical data are provided in Table 1. The rate of aneurysm rupture was 56% in never smokers vs 61% in current smokers. However, this relationship was not statistically significant (*P* = .26). The mean \pm SD age was 53.8 \pm 12.4 years. There was no significant difference in age between never smokers and current smokers (mean of 54.73 years never smokers vs 52.78 years current smokers, *P* = .27). There were 67 MCA aneurysms (34%), 56 ACoA aneurysms (28%), 49 PCoA aneurysms (25%), and 27 basilar tip aneurysms (14%). There were 154 women in the cohort, representing 77% of the total sample. There was no significant difference in the sex distribution between never smokers and current smokers with aneurysms. Among our cohort of patients with aneurysms, current smokers were more likely to have multiple aneurysms

(39%) than never smokers (25%, *P* = .04). There was no significant difference in the proportion of patients with hypertension or a family history of aneurysms between current smokers and never smokers.

Univariate statistical analysis of aneurysm intrinsic, transitional, and extrinsic morphological parameters is also provided in Table 2. There was no significant difference in aneurysm size as determined by the maximal diameter between never smokers (6.3 mm) and current smokers (6.6 mm, *P* = .63). Aneurysms in smokers were correlated with smaller volumes (299 mm³ in never smokers vs 246 mm³ in current smokers). However, this relationship was not statistically significant (*P* = .65). Smaller adjusted parent vessel diameters were also found in smokers (1.02 in never smokers vs 0.96 in current smokers, *P* = .03). There were no other significant differences in other metrics or vessel angles between nonsmoking and smoking patients using univariate analysis.

Our multivariate analysis included several known risk factors for aneurysm formation and rupture along with the aforementioned morphological parameters (Table 3). This allows us to find differences in parameters between never smokers and current smokers that were independent of known risk factors. For the variables included in the multivariate analysis, there were missing data for the following variables: volume (*n* = 8), hypertension (*n* = 1), and family history (*n* = 9). Current smokers were twice as likely to have multiple aneurysms as never smokers in a relationship that was statistically significant (OR: 2.15, *P* = .03). Current smokers were also more likely to have larger daughter vessel diameters (OR: 3.31, *P* = .01) and size ratios (OR: 1.78, *P* = .01). Finally, smokers were significantly more likely to have basilar apex aneurysms than nonsmokers (OR: 6.26, *P* = .02). When normalized parameters were used for the parent vessel diameter, daughter vessel diameter, flow angle, and parent-daughter angle, larger daughter vessel diameters (OR: 18.60, *P* = .004) and larger size ratios (OR: 1.74, *P* = .010) remained significant, whereas basilar apex location (OR: 3.02, *P* = .07) and

	Never Smokers (n = 102)	Current Smokers (n = 97)	P Value
Aneurysm rupture, no. (%)	56 (54.90)	61 (62.89)	.26
Age, y, mean (SD)	54.73 (12.97)	52.78 (11.79)	.27
Female, no. (%)	79 (77.45)	75 (77.32)	.98
Hypertension, no. (%)	58 (56.86)	42 (43.75)	.07
Multiple aneurysms, no. (%)	26 (25.49)	38 (39.18)	.04 ^b
Family history, no. (%)	13 (13.00)	15 (16.30)	.52
Type, no. (%)			
MCA	38 (37.25)	29 (29.90)	.27
ACoA	33 (32.35)	23 (23.71)	.18
PCoA	21 (20.59)	28 (28.87)	.18
BA	10 (9.80)	17 (17.53)	.12

^aMCA, middle cerebral artery; ACoA, anterior communicating artery; PCoA, posterior communicating artery; BA, basilar apex.

^bMCA, ACoA, PCoA, and BA.

TABLE 2. Univariate Analyses of Differences in the Morphological Parameters Between Smokers and Nonsmokers With Aneurysms^a

Metrics	Never Smokers, Mean (SD)	Current Smokers, Mean (SD)	P Value
Maximal diameter, mm	6.3 (4.9)	6.6 (3.2)	.635
Aneurysm volume, mm ³	299 (1024)	246 (531)	.65
Neck diameter, mm	5.2 (2.8)	4.8 (2.1)	.18
Aspect ratio	1.10 (0.79)	1.35 (1.52)	.14
Aneurysm angle	93.8 (22.5)	92.1 (25.7)	.95
Parent vessel diameters, mm	2.9 (0.8)	2.9 (0.7)	.92
Parent vessel diameters adjusted, mm	1.02 (0.21)	0.96 (0.17)	.03 ^a
Daughter diameters, mm	2.4 (0.7)	2.6 (0.8)	.26
Daughter diameters adjusted, mm	1.00 (0.19)	0.99 (0.26)	.80
Size ratio	2.5 (2.2)	2.9 (4.1)	.39
Angles			
Flow angles	112.7 (34.9)	107.5 (36.4)	.30
Daughter-daughter angles	117.1 (55.2)	111.8 (53.4)	.64
Parent-daughter angles	75.5 (27.1)	74.8 (26.6)	.86

^aSD, standard deviation.

smaller parent vessel diameter (OR: 0.15, $P = .06$) were nearly significant. Maximal aneurysm diameter was not included in our multivariate model because it is not completely independent of aspect ratio, size ratio, or volume. Daughter vessel angle was not included in the model because our data did not include daughter

vessel angle measurements for ACoA aneurysms. Aneurysm subtype ORs were compared with ACoA aneurysms.

DISCUSSION

Although the association between smoking and intracranial aneurysm formation and rupture has been well described, the mechanistic underpinnings of this relationship are not well understood. In this study, we examined the specific differences in aneurysm morphology between smokers and nonsmokers that may elucidate the effects of smoking on aneurysm formation and eventual rupture. The differences in morphological characteristics between smokers and nonsmokers suggest that smoking may create an altered environment for aneurysm formation. These differences, in turn, may affect the eventual rupture risk of the aneurysm.

Size ratio was first proposed by Dhar et al³² as a predictor of rupture risk in intracranial aneurysms, and there have been many studies that have sought to validate this finding in recent years,^{32,41-44} including morphological studies of rupture risk in our own cohort of ACoA aneurysms.²⁵ Intuitively, the association with size ratio implies that larger aneurysms arising from smaller vessels are more likely to rupture than smaller aneurysms arising from larger vessels. In terms of aneurysm genesis, size ratio captures the maximal deformation of the parent vessel achieved by the aneurysm and reflects the degree of aneurysm degradation of the vessel. Aneurysms arising in current smokers in our population were also significantly associated with larger size ratios (OR: 1.78, $P = .01$). Increased size ratio has been shown in a number of hemodynamic studies to lead to more complex intra-aneurysmal^{33,42,43,45,46} and aneurysmal^{45,47-49} vessel-related flow patterns that could influence the rates of both aneurysm formation and rupture. Our data suggest that smoking may contribute to the same morphological and hemodynamic

TABLE 3. Multivariate Analysis of Morphological Parameters Between Never Smokers and Current Smokers With Aneurysms^a

Variables	OR, Current Smokers vs Never Smokers (95% CI)	P Value
Age	0.99 (0.96-1.02)	.54
Female	0.78 (0.36-1.71)	.54
Multiple aneurysms	2.15 (1.07-4.42)	.03 ^b
Family history	1.21 (0.46-3.22)	.70
Hypertension	0.58 (0.29-1.17)	.13
Volume	1.00 (1-1)	.12
Neck diameter	0.85 (0.68-1.04)	.13
Aspect ratio	0.95 (0.50-1.79)	.87
Parent vessel diameter	0.54 (0.27-1.08)	.09
Daughter vessel diameter	3.13 (1.37-7.69)	.01 ^b
Size ratio	1.78 (1.16-2.77)	.01 ^b
Flow angle	1.00 (0.99-1.01)	.90
Parent-daughter vessel angle	1.00 (0.99-1.01)	.78
Aneurysm type (relative to ACoA)		
MCA	1.34 (0.57-3.22)	.51
PCoA	1.25 (0.33-4.72)	.74
BA	6.26 (1.46-29.53)	.02 ^b

^aMCA, middle cerebral artery; ACoA, anterior communicating artery; PCoA, posterior; BA, basilar apex; OR, odds ratio; CI, confidence interval.^bMCA, ACoA, PCoA, and BA.

conditions for aneurysm formation and may create a more favorable environment for aneurysm rupture.

Our finding that daughter vessel diameters are significantly larger in aneurysm patients who smoke (OR: 3.13, $P = .01$) may initially seem at odds with our size ratio findings because larger size ratios imply smaller vessels. Intuitively, aneurysm formation at a vessel branch point is much more likely to occur with smaller daughter vessel diameters because outflow velocities will be exponentially increased with a smaller radius of outflow through the daughter vessel, and these increased velocities would lead to the hemodynamic changes associated with aneurysm genesis⁴⁷⁻⁴⁹ and rupture.^{46,50,51} However, smoking is also associated with smaller parent vessel diameters, which, although not statistically significant, likely contributes to the larger size ratio. Moreover, the addition of physiological and biochemical changes associated with smoking may be more permissive of and accelerate aneurysm pathophysiology to allow formation to occur despite larger daughter vessel diameters.

In addition to absolute vessel diameters and angles, we had also normalized the parameters so that they are relative measures with respect to the average within each aneurysm type. Because each location in the vasculature is associated with different average sizes and angles, the normalization decreases the confounding secondary to location-specific characteristics. In our study, this normalization maintained the significance of both morphological parameters, size ratio and daughter vessel diameter, but increased the relative impact of daughter vessel diameter.

In our study, smokers with aneurysms were significantly more likely to have basilar apex aneurysms than nonsmokers with aneurysms (OR: 6.26). There have only been a few studies of location-specific associations of aneurysm development with clinical risk factors such as smoking. Several studies examine the clinical risk factors associated with posterior circulation aneurysms.^{23,26,52,53} Of these, only Lindner et al⁵² reported on clinical risk factors in basilar apex aneurysms. They identified a similar relationship in these aneurysms to smoking, in which patients who smoke were significantly more likely to have basilar apex aneurysms compared with nonsmokers with aneurysms, with no significant differences with regard to smoking in any other aneurysm location (OR: 3.3). Basilar apex aneurysms carry with them a higher risk of rupture, morbidity, and mortality.⁵⁴⁻⁵⁶ They also present significant management considerations in terms of neurosurgical approaches and techniques.⁵⁷⁻⁵⁹ Thus, the association between smoking and basilar apex aneurysm formation and rupture is significant and warrants further study.

Current smokers with aneurysms in our study were significantly more likely to have multiple aneurysms. Smoking is a well-known risk factor for de novo aneurysm formation,^{60,61} and in a recent prospective study of de novo aneurysm formation identified by routine delayed radiographic surveillance studies in patients with at least 1 previous intracranial aneurysm, smoking significantly increased the risk of de novo aneurysm formation (hazard ratio: 2.58, 95% CI: 1.13-5.90).⁶² Given that a significant number of de novo aneurysms present with rupture, the effects of smoking

on the morphology and hemodynamics of aneurysms presented in this study are likely predictive of both aneurysm formation and rupture.

Limitations

There are several limitations to this study that should be acknowledged. First, smoking in our study was defined as current smokers. There was no specific determination of the relationship of pack-years with the variables studied; thus, the dynamic effects of increasing degrees of smoking are not well captured in our results. Because of the retrospective case-control design of this study, most patients (except for those with basilar apex aneurysms) were treated either surgically or endovascularly, and the study population is inherently biased toward morphologically “dangerous”-appearing lesions. This may limit the applicability of our data to general aneurysm patients in whom there is less clinical equipoise about treatment. Also, the effect that aneurysm rupture and subsequent hemorrhage may have on aneurysm geometry was not taken in account, although several studies suggested that rupture does not significantly alter aneurysm morphology.³¹⁻³³

CONCLUSION

Research linking the effects of smoking on aneurysm formation and rupture risk has largely focused on potential biochemical and biomechanical mechanisms. However, in addition to physiological conditions (such as flow rate and blood viscosity), aneurysm hemodynamics are mostly directly influenced by aneurysm and vascular morphology, which we have shown in the present study is significantly more altered in the smoking population of patients with aneurysms. There were several aspects of aneurysm morphology significantly associated with smoking status including larger daughter vessel diameters, larger size ratio, and location at the basilar apex. Future study on how these specific morphological changes may influence aneurysmal hemodynamics may provide the morphological basis for how smoking leads to increased aneurysm formation and rupture. Understanding of these morphological changes may allow clinicians to more accurately determine rupture risk in smokers and counsel/treat accordingly.

Disclosures

This work was supported by the Daniel E. Ponton Fund (R.D.) and the American Heart Association Scholarship in Cerebrovascular Disease and Stroke (A.H.). A portion of these data was presented as a poster at the International Stroke Conference in 2013. The authors have no personal, financial, or institutional interest in any of the drugs, materials, or devices described in this article.

REFERENCES

1. Gabriel RA, Kim H, Sidney S, et al. Ten-year detection rate of brain arteriovenous malformations in a large, multiethnic, defined population. *Stroke*. 2010;41(1):21-26.
2. Vlak MH, Algra A, Brandenburg R, Rinkel GJ. Prevalence of unruptured intracranial aneurysms, with emphasis on sex, age, comorbidity, country, and time period: a systematic review and meta-analysis. *Lancet Neurol*. 2011;10(7):626-636.
3. Kikuchi K, Tancharoen S, Ito T, et al. Potential of the angiotensin receptor blockers (ARBs) telmisartan, irbesartan, and candesartan for inhibiting the

- HMGB1/RAGE axis in prevention and acute treatment of stroke. *Int J Mol Sci*. 2013;14(9):18899-18924.
4. Iguchi Y, Kimura K, Sone K, et al. Stroke incidence and usage rate of thrombolysis in a Japanese urban city: the Kurashiki stroke registry. *J Stroke Cerebrovasc Dis*. 2013;22(4):349-357.
 5. Takai J, Santu A, Zheng H, et al. Laminar shear stress upregulates endothelial Ca²⁺-activated K⁺ channels KCa2.3 and KCa3.1 via a Ca²⁺/calmodulin-dependent protein kinase/Akt/p300 cascade. *Am J Physiol Heart Circ Physiol*. 2013;305(4):H484-H493.
 6. Miura Y, Ishida F, Umeda Y, et al. Low wall shear stress is independently associated with the rupture status of middle cerebral artery aneurysms. *Stroke*. 2013;44(2):519-521.
 7. Sadatomo T, Yuki K, Migita K, Imada Y, Kuwabara M, Kurisu K. Differences between middle cerebral artery bifurcations with normal anatomy and those with aneurysms. *Neurosurg Rev*. 2013;36(3):437-445.
 8. Kissela BM, Sauerbeck L, Woo D, et al. Subarachnoid hemorrhage: a preventable disease with a heritable component. *Stroke*. 2002;33(5):1321-1326.
 9. Broderick JP, Viscoli CM, Brott T, et al. Major risk factors for aneurysmal subarachnoid hemorrhage in the young are modifiable. *Stroke*. 2003;34(6):1375-1381.
 10. Singh PK, Marzo A, Howard B, et al. Effects of smoking and hypertension on wall shear stress and oscillatory shear index at the site of intracranial aneurysm formation. *Clin Neurol Neurosurg*. 2010;112(4):306-313.
 11. Adamson J, Humphries SE, Ostergaard JR, Voldby B, Richards P, Powell JT. Are cerebral aneurysms atherosclerotic? *Stroke*. 1994;25(5):963-966.
 12. Inci S, Spetzler RF. Intracranial aneurysms and arterial hypertension: a review and hypothesis. *Surg Neurol*. 2000;53(6):530-540; discussion 540-542.
 13. Schievink WI, Prakash UB, Piepgras DG, Mokri B. Alpha 1-antitrypsin deficiency in intracranial aneurysms and cervical artery dissection. *Lancet*. 1994;343(8895):452-453.
 14. Greenhalgh RM, Laing S, Taylor GW. Risk factors in carotid artery stenosis and intracranial aneurysms. *J Cardiovasc Surg (Torino)*. 1980;21(5):559-567.
 15. Burleson AC, Turitto VT. Identification of quantifiable hemodynamic factors in the assessment of cerebral aneurysm behavior. On behalf of the Subcommittee on Biorheology of the Scientific and Standardization Committee of the ISTH. *Thromb Haemost*. 1996;76(1):118-123.
 16. Gao L, Hoi Y, Swartz DD, Kolega J, Siddiqui A, Meng H. Nascent aneurysm formation at the basilar terminus induced by hemodynamics. *Stroke*. 2008;39(7):2085-2090.
 17. Morimoto M, Miyamoto S, Mizoguchi A, Kume N, Kita T, Hashimoto N. Mouse model of cerebral aneurysm: experimental induction by renal hypertension and local hemodynamic changes. *Stroke*. 2002;33(7):1911-1915.
 18. Sacco RL, Wolf PA, Bharucha NE, et al. Subarachnoid and intracerebral hemorrhage: natural history, prognosis, and precursive factors in the Framingham Study. *Neurology*. 1984;34(7):847-854.
 19. Gonzalez CF, Cho YI, Ortega HV, Moret J. Intracranial aneurysms: flow analysis of their origin and progression. *AJNR Am J Neuroradiol*. 1992;13(1):181-188.
 20. de Simone G, Devereux RB, Chinali M, Best LG, Lee ET, Welty TK. Association of blood pressure with blood viscosity in American Indians: the Strong Heart Study. *Hypertension*. 2005;45(4):625-630.
 21. Price JF, Mowbray PI, Lee AJ, Rumley A, Lowe GD, Fowkes FG. Relationship between smoking and cardiovascular risk factors in the development of peripheral arterial disease and coronary artery disease: Edinburgh Artery Study. *Eur Heart J*. 1999;20(5):344-353.
 22. Lin N, Ho A, Gross BA, et al. Differences in simple morphological variables in ruptured and unruptured middle cerebral artery aneurysms. *J Neurosurg*. 2012;117(5):913-919.
 23. Matsukawa H, Fujii M, Akaike G, et al. Morphological and clinical risk factors for posterior communicating artery aneurysm rupture. *J Neurosurg*. 2014;120(1):104-110.
 24. Matsukawa H, Uemura A, Fujii M, Kamo M, Takahashi O, Sumiyoshi S. Morphological and clinical risk factors for the rupture of anterior communicating artery aneurysms. *J Neurosurg*. 2013;118(5):978-983.
 25. Lin N, Ho A, Charoenvimolphan N, Frerichs KU, Day AL, Du R. Analysis of morphological parameters to differentiate rupture status in anterior communicating artery aneurysms. *PLoS One*. 2013;8(11):e79635.
 26. Ho A, Lin N, Charoenvimolphan N, et al. Morphological parameters associated with ruptured posterior communicating aneurysms. *PLoS One*. 2014;9(4):e94837.
 27. Sadatomo T, Yuki K, Migita K, Taniguchi E, Kodama Y, Kurisu K. Evaluation of relation among aneurysmal neck, parent artery, and daughter arteries in middle cerebral artery aneurysms, by three-dimensional digital subtraction angiography. *Neurosurg Rev*. 2005;28(3):196-200.
 28. Sadatomo T, Yuki K, Migita K, Taniguchi E, Kodama Y, Kurisu K. The characteristics of the anterior communicating artery aneurysm complex by three-dimensional digital subtraction angiography. *Neurosurg Rev*. 2006;29(3):201-207.
 29. Pieper S, Halle M, Kikinis R. 3D SLICER. *Proc IEEE Int Symp Biomed Imaging*. 2004;1:632-635.
 30. Pieper S, Lorenzen B, Schroeder W, Kikinis R. The NA-MIC kit: ITK, VTK, pipelines, grids and 3D Slicer as an open platform for the medical image computing community. *Proc IEEE Int Symp Biomed Imaging*. 2006;1:698-701.
 31. Raghavan ML, Ma B, Harbaugh RE. Quantified aneurysm shape and rupture risk. *J Neurosurg*. 2005;102(2):355-362.
 32. Dhar S, Tremmel M, Mocco J, et al. Morphology parameters for intracranial aneurysm rupture risk assessment. *Neurosurg Rev*. 2008;32(2):185-196; discussion 196-197.
 33. Ujii H, Tamano Y, Sasaki K, Hori T. Is the aspect ratio a reliable index for predicting the rupture of a saccular aneurysm? *Neurosurgery*. 2001;48(3):495-502; discussion 502-503.
 34. Ho AL, Mouminah A, Du R. Posterior cerebral artery angle and the rupture of basilar tip aneurysms. *PLoS One*. 2014;9(10):e110946.
 35. Ma B, Harbaugh RE, Raghavan ML. Three-dimensional geometrical characterization of cerebral aneurysms. *Ann Biomed Eng*. 2004;32(2):264-273.
 36. Parlea L, Fahrig R, Holdsworth DW, Lownie SP. An analysis of the geometry of saccular intracranial aneurysms. *AJNR Am J Neuroradiol*. 1999;20(6):1079-1089.
 37. Ujii H, Tachibana H, Hiramoto O, et al. Effects of size and shape (aspect ratio) on the hemodynamics of saccular aneurysms: a possible index for surgical treatment of intracranial aneurysms. *Neurosurgery*. 1999;45(1):119-129; discussion 129-130.
 38. Ma D, Tremmel M, Paluch RA, Levy EI, Meng H, Mocco J. Size ratio for clinical assessment of intracranial aneurysm rupture risk. *Neural Res*. 2010;32(5):482-486.
 39. Baharoglu MI, Schirmer CM, Hoit DA, Gao BL, Malek AM. Aneurysm inflow-angle as a discriminant for rupture in sidewall cerebral aneurysms: morphometric and computational fluid dynamic analysis. *Stroke*. 2010;41(7):1423-1430.
 40. Ford MD, Lee SW, Lownie SP, Holdsworth DW, Steinman DA. On the effect of parent-aneurysm angle on flow patterns in basilar tip aneurysms: towards a surrogate geometric marker of intra-aneurysmal hemodynamics. *J Biomech*. 2008;41(2):241-248.
 41. Rahman M, Smietana J, Hauck E, et al. Size ratio correlates with intracranial aneurysm rupture status: a prospective study. *Stroke*. 2010;41(5):916-920.
 42. Tremmel M, Dhar S, Levy EI, Mocco J, Meng H. Influence of intracranial aneurysm-to-parent vessel size ratio on hemodynamics and implication for rupture: results from a virtual experimental study. *Neurosurgery*. 2009;64(4):622-630; discussion 630-631.
 43. Xiang J, Natarajan SK, Tremmel M, et al. Hemodynamic-morphologic discriminants for intracranial aneurysm rupture. *Stroke*. 2011;42(1):144-152.
 44. Ryu CW, Kwon OK, Koh JS, Kim EJ. Analysis of aneurysm rupture in relation to the geometric indices: aspect ratio, volume, and volume-to-neck ratio. *Neuroradiology*. 2011;53(11):883-889.
 45. Long Y, Yu H, Zhuo Z, et al. A geometric scaling model for assessing the impact of aneurysm size ratio on hemodynamic characteristics. *Biomed Eng Online*. 2014;13:17.
 46. Meng H, Wang Z, Hoi Y, et al. Complex hemodynamics at the apex of an arterial bifurcation induces vascular remodeling resembling cerebral aneurysm initiation. *Stroke*. 2007;38(6):1924-1931.
 47. Malek AM, Alper SL, Izumo S. Hemodynamic shear stress and its role in atherosclerosis. *JAMA*. 1999;282(21):2035-2042.
 48. Nam D, Ni CW, Rezvan A, et al. Partial carotid ligation is a model of acutely induced disturbed flow, leading to rapid endothelial dysfunction and atherosclerosis. *Am J Physiol Heart Circ Physiol*. 2009;297(4):H1535-H1543.
 49. Barakat AI, Davies PF. Mechanisms of shear stress transmission and transduction in endothelial cells. *Chest*. 1998;114(1 suppl):58S-63S.
 50. Shojima M, Oshima M, Takagi K, et al. Magnitude and role of wall shear stress on cerebral aneurysm: computational fluid dynamic study of 20 middle cerebral artery aneurysms. *Stroke*. 2004;35(11):2500-2505.
 51. Kaiser D, Freyberg MA, Friedl P. Lack of hemodynamic forces triggers apoptosis in vascular endothelial cells. *Biochem Biophys Res Commun*. 1997;231(3):586-590.
 52. Lindner SH, Bor AS, Rinkel GJ. Differences in risk factors according to the site of intracranial aneurysms. *J Neurol Neurosurg Psychiatry*. 2010;81(1):116-118.

53. Eftekhari B, Morgan MK. Preoperative factors affecting the outcome of unruptured posterior circulation aneurysm surgery. *J Clin Neurosci*. 2011;18(1):85-89.
54. Molyneux A, Kerr R; International Subarachnoid Aneurysm Trial (ISAT) Collaborative Group, et al. International Subarachnoid Aneurysm Trial (ISAT) of neurosurgical clipping versus endovascular coiling in 2143 patients with ruptured intracranial aneurysms: a randomized trial. *J Stroke Cerebrovasc Dis*. 2002;11(6):304-314.
55. Unruptured intracranial aneurysms—risk of rupture and risks of surgical intervention. International Study of Unruptured Intracranial Aneurysms Investigators. *N Engl J Med*. 1998;339(24):1725-1733.
56. Wiebers DO, Whisnant JP, Huston J III, et al. Unruptured intracranial aneurysms: natural history, clinical outcome, and risks of surgical and endovascular treatment. *Lancet*. 2003;362(9378):103-110.
57. Gnanalingham KK, Apostolopoulos V, Barazi S, O'Neill K. The impact of the international subarachnoid aneurysm trial (ISAT) on the management of aneurysmal subarachnoid haemorrhage in a neurosurgical unit in the UK. *Clin Neurol Neurosurg*. 2006;108(2):117-123.
58. Lai L, Morgan MK. The impact of changing intracranial aneurysm practice on the education of cerebrovascular neurosurgeons. *J Clin Neurosci*. 2012;19(1):81-84.
59. Qureshi AI, Vazquez G, Tariq N, Suri MF, Lakshminarayan K, Lanzino G. Impact of International Subarachnoid Aneurysm Trial results on treatment of ruptured intracranial aneurysms in the United States. Clinical article. *J Neurosurg*. 2011;114(3):834-841.
60. Juvela S, Poussa K, Porras M. Factors affecting formation and growth of intracranial aneurysms: a long-term follow-up study. *Stroke*. 2001;32(2):485-491.
61. Wermer MJ, van der Schaaf IC, Velthuis BK, Algra A, Buskens E, Rinkel GJ. Follow-up screening after subarachnoid haemorrhage: frequency and determinants of new aneurysms and enlargement of existing aneurysms. *Brain*. 2005;128(pt 10):2421-2429.
62. Lai LT, Morgan MK, Patel NJ. Smoking increases the risk of de novo intracranial aneurysms. *World Neurosurg*. 2014;82(1-2):e195-e201.

COMMENT

The authors present an interesting analysis looking at associations between smoking status and aneurysm location and morphology. The

aspects of aneurysm location and morphology that were significantly associated with smoking status—larger daughter vessel diameters, larger size ratio, and location at the basilar apex—are of interest with regard to explaining why smokers may have a higher risk of rupture. As noted by the authors, the relationship between wall shear stress and aneurysm rupture is a complicated one. The ability to quantify aneurysm size and shape and to determine how these geometric features affect aneurysm hemodynamics and biology have become important tools in the attempt to understand how aneurysms develop and grow and to predict the natural history risks for individual patients with intracranial aneurysms.¹⁻⁷

Robert E. Harbaugh
Hershey, Pennsylvania

1. Laaksamo E, Ramachandran M, Frosen J, et al. Intracellular signaling pathways and size, shape, and rupture history of human intracranial aneurysms. *Neurosurgery*. 2012;70(6):1565-1573.
2. Ma B, Lu J, Harbaugh RE, Raghavan ML. Nonlinear, anisotropic stress analysis of anatomically realistic cerebral aneurysms. *J Biomed Eng*. 2007;129(1):88-96.
3. Ma B, Harbaugh RE, Raghavan ML. Three-dimensional geometrical characterization of cerebral aneurysms. *Ann Biomed Eng*. 2004;32(2):264-273.
4. Raghavan M, Ma B, Harbaugh RE. Quantified aneurysm shape and rupture risk. *J Neurosurg*. 2005;102(2):355-362.
5. Ramachandran M, Laakso A, Harbaugh RE, Raghavan ML. On the role of modeling choices in estimation of cerebral aneurysm wall tension. *J Biomech*. 2012;45(16):2914-2919.
6. Retarekar R, Ramachandran M, Berkowitz B, et al. Stratification of a population of intracranial aneurysms using blood flow metrics. *Comput Methods Biomech Biomed Engin*. 2013;18(10):1072-1082.
7. Zhou X, Raghavan ML, Harbaugh RE, Lu J. Patient-specific wall stress analysis in cerebral aneurysms using inverse shell model. *Ann Biomed Eng*. 2010;38(2):478-489.